

1 **Accepted for Publication**

2

3 **THE EFFECTS OF 8 WEEKS VOLUNTARY WHEEL RUNNING ON THE**
4 **CONTRACTILE PERFORMANCE OF ISOLATED LOCOMOTORY (SOLEUS) AND**
5 **RESPIRATORY (DIAPHRAGM) SKELETAL MUSCLE DURING EARLY AGEING**

6

7 Jason Tallis¹ (✉), Matthew F. Higgins², Frank Seebacher³, Val M. Cox¹, Michael J. Duncan¹,
8 Rob S. James¹

9

10 ¹School of Life Sciences, James Starley Building, Coventry University, Priory Street,
11 Coventry CV1 5FB, UK

12

13 ² Department of Sport, Outdoor and Exercise Science, Derby University, Kedleston Road,
14 Derby, DE22 1GB, UK

15

16 ³School of Biological Sciences, A08 University of Sydney, Science Road, Sydney, NSW,
17 2006, Australia

18

19 Email: tallisj2@uni.coventry.ac.uk

20

21

22

23

24

25

26

27

28

29 **ABSTRACT**

30 Decreased skeletal muscle performance with increasing age is strongly associated with reduced
31 mobility and quality of life. Increased physical activity is a widely prescribed method of
32 reducing the detrimental effects of ageing on skeletal muscle contractility. The present study
33 uses isometric and work loop testing protocols to uniquely investigate the effects of 8 weeks of
34 voluntary wheel running on the contractile performance of isolated dynapenic soleus and
35 diaphragm muscles of 38 week old CD1 mice. When compared to untrained controls, voluntary
36 wheel running induced significant improvements in maximal isometric stress and work loop
37 power, a reduced resistance to fatigue, but greater cumulative work during fatiguing work loop
38 contractions in isolated muscle. These differences occurred without appreciable changes in
39 LDH, CS, SERCA or MHC expression synonymous with this form of training in younger
40 rodent models. Despite the given improvement in contractile performance, the average running
41 distance significantly declined over the course of the training period, indicating that this form
42 of training may not be sufficient to fully counteract the longer term ageing induced decline in
43 skeletal muscle contractile performance. Although these results indicate that regular low
44 intensity physical activity may be beneficial in offsetting the age-related decline in skeletal
45 muscle contractility, the present findings infer that future work focusing on the maintenance of
46 a healthy body mass with increasing age and its effects on myosin-actin cross bridge kinetics
47 and Ca^{2+} handling, is needed to clarify the mechanisms causing the improved contractile
48 performance in trained dynapenic skeletal muscle.

49
50 **KEY WORDS:** Dynapenia, Training, Contractile Performance, Weight Management,
51 Sarcopenia

52

53

54

55

56

57 **INTRODUCTION**

58 An age-related reduction in mobility and quality of life is associated with a decrease in the
59 contractile performance of skeletal muscle (Williams et al., 2002, Landi et al., 2012, Woo et
60 al., 2016). As such, older adults are encouraged to engage in regular physical activity to offset
61 degenerative changes in muscle contractility (WHO, 2017, Marcell, 2003, Iolascon et al.,
62 2014). Although *in vivo* evidence is rife with studies reporting training induced improvements
63 in the maximal strength and power of older adults (Pyka et al., 1994, McCartney et al., 1995,
64 Mayer et al., 2011, Melov et al., 2007, Seguin and Nelson, 2003, Reid et al., 2008, Reid et al.,
65 2015), fewer studies have examined training responses during the onset of muscle ageing,
66 which has been shown to occur relatively early on in life (Lexell, 1995). Given that
67 mechanistically the age associated decline in muscle contractility has been attributed to
68 processes both integral to the muscle and the wider body (Doherty, 2003), work is needed to
69 distinguish the effect of training directly on skeletal muscle. The present study uses an *in vitro*
70 isolated skeletal muscle approach to examine the effects of voluntary wheel running on muscle
71 contractility in rodents at the early stages of the muscle ageing process.

72

73 Previous work examining isolated skeletal muscle contractility in aged rodent models (Brooks
74 and Faulkner, 1988, Gonzalez et al., 2000, Zhang and Kelsen, 1990) has provided a vital
75 contribution to our understanding of the muscle ageing response. Only very recently however,
76 have such models been employed to investigate the effects of early ageing on muscle
77 contractility (Tallis et al., 2014b). Work by our research group using an inbred strain of female
78 CD-1 mice has demonstrated that contractile performance has significantly declined by 30
79 weeks of age. There is a distinct dearth of evidence exploring the effect of training on skeletal
80 muscle plasticity during early ageing; having a better understanding of the training adaptations
81 that occur at this time may prove important for understanding and reducing the more severe
82 reduction in muscle contractility that occurs during the onset of sarcopenia in older ageing.

83

84 Examining training-induced changes in the contractile performance of isolated skeletal muscle
85 allows muscle specific changes in contractility to be determined. *In vivo* assessments of muscle
86 function are largely performed using gross motor skills, and consequently, require the
87 recruitment of muscle groups. Due to variations in cross sectional area, architecture and fibre
88 type composition, it is difficult to ascertain the muscle-specific contractile response.
89 Furthermore, the sequence of electrical (central nervous system) and mechanical processes
90 involved with force production make it difficult to determine the magnitude of any training-
91 induced benefits at the muscle level. Previous *in vivo* work, examining training effects on
92 muscle contractility, report gains in absolute muscle force and power (Pyka et al., 1994,
93 McCartney et al., 1995, Mayer et al., 2011, Melov et al., 2007, Seguin and Nelson, 2003, Reid
94 et al., 2008, Reid et al., 2015), which tells us very little about muscle contractility relative to
95 size. Importantly, assessment of contractile performance using isolated muscle allows muscle
96 quality to be determined (measure of force or power relative to muscle size, Tallis et al., 2017).
97 A training-induced increase in muscle quality would be more desirable than an increase in
98 muscle mass. Muscle producing high force and power in a lower quantity of tissue (i.e. good
99 muscle quality) would reduce tissue maintenance cost and body mass, thus reducing the force
100 that must be produced by the musculature to overcome inertia of the body.

101
102 Irrespective of age, studies that have examined skeletal muscle adaptions to training have
103 primarily focused on results from biochemical analysis to quantify changes in fibre type
104 composition, metabolic capacity and vascular adaptations (Brown et al., 1992, Sullivan et al.,
105 1995, Houle-Leroy et al., 2000, Allen et al., 2001, Behnke et al., 2012). Surprisingly, only a
106 very small number of studies have examined the effect of physical training on isolated skeletal
107 muscle contractility, with equivocal findings (Taylor et al., 1976, Metzger and Fitts, 1986,
108 Carter et al., 1995, Zhan et al., 1999, Ergen et al., 2005, Willems and Stauber, 2000, Hayes and
109 Williams, 1996). The ambiguity in research findings can likely be attributed to differences in
110 gender, age, strain and species of animals, method and duration of training, and experimental
111 protocol used to measure skeletal muscle contractility.

Such previous assessments of isolated muscle function examine contractility using isometric and isovelocity methods which have poor relevance to *in vivo* muscle function where cyclical power producing contractions are performed (Josephson, 1985, James et al., 1995). As such, the present study will use the work loop technique to uniquely examine the effect of training using a methodological approach that better approximates *in vivo* muscle function (Josephson, 1985). Like *in vivo* contractile function, this method considers the interaction between force produced during shortening, passive resistance to stretch, and influence of activation and relaxation rates, using waveforms and stimulation patterns that more closely replicate *in vivo* patterns (James et al., 1995, James et al., 1996, Tallis et al., 2014b, Josephson, 1985). Other assessments of muscle contractility fail to consider the interaction of these important mechanical characteristics, and a change in one or a combination of these factors could have profound effects on peak power and fatigue resistance that may not be demonstrated accurately using other methods. Furthermore, previous assessments of training-induced changes in muscle power have been derived from isovelocity assessments of muscle contractility (Zhan et al., 1999) which substantially overestimate the power output measured by the work loop technique (James et al., 1996).

The aim of the present study was to examine the effects of voluntary wheel running on the contractile properties of soleus and diaphragm muscle isolated from 38 week old CD-1 mice. Given that previous work has demonstrated that the onset of muscle ageing occurs by 30 weeks of age in these muscles, for this strain of mice (Tallis et al., 2014b), the present work offers an important insight into skeletal muscle plasticity during the initial stages of the ageing process. The soleus muscle has an important role in locomotion (James et al., 1995, Nicolopoulos-Stournaras and Iles, 1984) and postural control. Voluntary wheel running has been demonstrated to increase the proportion of slow oxidative fibres in young mice (Allen et al., 2001), and promote hypertrophy of the soleus in both young and old rats (Brown et al., 1992). Despite this evidence, it is not clear how voluntary wheel running will directly affect soleus contractility. Furthermore, there is a wealth of literature outlining the benefits of low intensity,

140 long duration exercise training on ventilatory performance (Sheel, 2002). However given the
141 importance of the diaphragm muscle in pulmonary function, there is a dearth of research that
142 considers the effects of training on the contractile function of this muscle (Sheel, 2002). It was
143 hypothesised that voluntary wheel running would evoke improved force, power and fatigue
144 resistance of both the soleus and diaphragm, which would be underpinned by a greater muscle
145 mass, shift to a slower fibre type and an increased oxidative capacity.

146

147

148

149

150

151

152

153

154

155

156

157

158

159

160

161

162

163

164

165

166

167

168 **Method**

169

170 *Animals & Training*

171

172 The ethics committee of Coventry University approved the use of animals in this study. Female
173 white mice (strain CD1, Charles River, UK) were bred and kept in house at Coventry
174 University. From birth, and throughout the duration of the experiment, animals had *ad libitum*
175 access to food (CRM(P); SDS/Dietex International Ltd) and water, and were kept in 12:12
176 light:dark cycles at 50% relative humidity. For the first 30 weeks animals were kept in groups
177 of 8 without access to running wheels. Previous work by our group has indicated that the
178 greatest early ageing related decline in skeletal muscle contractile performance in female CD1
179 mice occurs between 30-50 weeks (Tallis et al., 2014b), and we therefore used 38 week old
180 mice to examine the effects of training on the early ageing response. At 30 weeks of age,
181 animals were weighed to the nearest 0.1 g and randomly divided into a training group and a
182 control group (n=14 in each group; body mass 45 ± 2 g and 43 ± 1 g for training and control group
183 respectively; t-test p=0.23). For the duration of the experiment, mice in both the control and
184 treatment groups were housed in individual cages. Each mouse in the training group had access
185 to a running wheel (diameter = 15cm) for 8 weeks, with revolutions recorded either every 30
186 minutes (n= 7) or every 24 hours (n= 7). We monitored the activity of a subset of training group
187 animals at 30 minute intervals to more closely determine the daily variation in activity. Running
188 wheels were locked 24-48 hours prior to assessment of the contractile and biochemical
189 properties of the target skeletal muscle. For the duration of the experiments control animals
190 were housed in identical conditions without access to running wheels.

191

192 *Dissection*

193

194 The dissection procedure and assessment of mechanical properties were carried out according
195 to published protocols (James et al., 2005, Higgins et al., 2013, Tallis et al., 2012, Tallis et al.,

196 2014b). Animals were sacrificed by cervical dislocation, in accordance with British Home
197 Office Animals (Scientific Procedures) Act 1986, Schedule 1, and then weighed to determine
198 body mass. Both hind limbs or the thoracic cavity were rapidly removed from the animal at
199 room temperature (19-21°C), and throughout the dissection process were kept in regularly
200 changed, cooled (1-4°C), oxygenated (95% O₂; 5% CO₂) Krebs-Henseleit solution
201 (composition in mM: NaCl 118; KCl 4.75; MgSO₄ 1.18; NaHCO₃ 24.8; KH₂PO₄ 1.18; glucose
202 10; CaCl₂ 2.54; pH 7.55, at room temperature prior to oxygenation). Soleus muscle was used
203 to serve as an indicator of locomotor muscle adaptations and diaphragm as an indicator of
204 changes in pulmonary function.

205

206 Soleus muscle from the left hind limb was isolated and frozen immediately in liquid nitrogen,
207 then stored in a -80°C freezer for later biochemical analysis. Soleus muscle from the right hind
208 limb was then isolated and pinned out at approximately its resting length, and aluminium foil
209 T clips were placed around both the proximal and distal tendons. The T-clips were used to
210 prevent tendon slippage during muscle activation and allow attachment of the muscle
211 preparation to the custom designed muscle rig. Whole diaphragm muscle was dissected, but
212 only a ventral section of the costal diaphragm was used in the protocol to analyse contractile
213 performance of muscle. Aluminium foil T-clips were wrapped around the central tendon at one
214 end, and at the opposing end two ribs anchoring the muscle were left intact, and the T-clip and
215 the ribs were used to attach the muscle preparation to the muscle rig. The left half of the
216 diaphragm was dissected and frozen in liquid nitrogen.

217

218 *Assessment of Contractile Properties*

219

220 One end of each muscle was attached to a force transducer (UF1, Piodes Controls), and the
221 opposite end to a motor arm (V201, Ling Dynamic Systems) to control length changes. Position
222 of the motor arm was determined by a Linear Variable Displacement Transformer (DFG5.0,
223 Solartron Metrology). Temperature in the muscle chamber was maintained at 37 ± 0.2°C

224 throughout the duration of the protocol. Prior to assessment of contractile properties, each
225 muscle preparation was left in the muscle chamber for 10 minutes to equilibrate to the new
226 environment. Initially each muscle was subjected to a series of isometric twitches while
227 stimulation amplitude (usually 12-16 V & 10-16V for soleus & diaphragm respectively: current
228 fixed at 160mA) and length were optimised to produce a maximal twitch force response.

229

230 At the predetermined optimal length for twitch force, each muscle preparation was subjected to
231 a series of stimulations, and stimulation frequency was optimised (usually 140Hz for both
232 soleus & diaphragm) at a fixed burst duration (350 ms & 250 ms for soleus & diaphragm
233 respectively) to evoke maximal tetanic force. Time to half peak tetanus (THPT) and time from
234 last stimulus to half tetanus relaxation (LSHR) were measured as indicators of muscle
235 activation and relaxation time, respectively. The muscle length that corresponded to maximal
236 isometric stress was measured using an eyepiece graticule fitted to a dissection microscope, and
237 was defined as L_0 . 85% of the measured muscle length was used as an estimate of fibre length
238 for soleus, in line with previous research (James et al., 1995). No such estimates of fibre length
239 have been reported for diaphragm so the physical length measured was used as L_0 , as in
240 previous work (Tallis et al., 2014b). An interval of 5 minutes was given between tetanic
241 stimulations in order to allow sufficient muscle recovery time.

242

243 Muscle power output was assessed using the work loop technique. Here each muscle was
244 subjected to a symmetrical sinusoidal length change waveform around the previously
245 determined L_0 . A typical strain of 0.10 was used and the muscle was electrically stimulated
246 during shortening using the optimised stimulation amplitude and frequency parameters that
247 yielded maximal isometric force. Put simply, the muscle was stretched by 5% of L_0 whilst
248 passive, then shortened by 10%, and was then lengthened by 5% back to L_0 . Instantaneous
249 power output was calculated for every data point in each work loop (10,000 data points per
250 work loop) by multiplying instantaneous velocity by instantaneous force. Instantaneous power

251 output values were averaged across the entire length change cycle to generate an average power
252 output for each length change cycle.

253

254 A cycle frequency of 5Hz and 7Hz was used for soleus and diaphragm muscle, respectively,
255 concurrent with previous research which found that these cycle frequencies elicit maximal
256 power output in these muscles (Altringham and Young, 1991, James et al., 1995, Tallis et al.,
257 2012, Askew and Marsh, 1997). The cycle frequencies chosen have been found to elicit
258 maximal power output in mice of this age and strain (authors, unpublished work). Furthermore,
259 these cycle frequencies are attainable *in vivo* (James et al., 1995). The strain of 0.10 was based
260 on previous estimations of the strain required for production of maximal power in both soleus
261 and diaphragm (James et al., 2005, Altringham and Young, 1991). Stimulation parameters were
262 then adjusted to optimise net work. The duration of electrical stimulation during the shortening
263 phase was further optimised to evoke maximal net work. 65 and 55 ms burst durations were
264 used for soleus and diaphragm, respectively, as described in previous work (James et al., 1995,
265 James et al., 1996, Tallis et al., 2014a). On occasions the burst duration had to be altered to
266 adjust the number of stimuli given in order to maximise muscle power output of individual
267 muscle preparations. The alteration in stimulation duration was determined by examining the
268 maximal work loop power output and by interpretation of the work loop shapes. A stimulation
269 phase shift, which is the period of time before the onset of the shortening that stimulation
270 begins, of -10ms and -5ms was used for soleus and diaphragm, respectively, in order to elicit
271 maximal net work (Tallis et al., 2014b).

272

273 The magnitude and frequency of length changes and electrical stimulation were controlled via
274 custom written software (Testpoint, CEC) via a D/A board (KPCI3108, Keithley Instruments).
275 Each muscle was subjected to a set of four sinusoidal length change cycles at 10-minute
276 intervals until maximal muscle power output was achieved. The third work loop, of each set of
277 four, typically produced the highest power and was therefore taken as the indicative measure
278 of muscle power output in all work loop experiments.

279 Fatigue of muscle power output was tested by subjecting the muscle to 100 consecutive work
280 loops at the previously determined optimal parameters for maximal power output. Power output
281 was recorded for every second work loop, and the time for power to fall below 50% of the pre-
282 fatigue maximum was used to indicate fatigue resistance. Cumulative net work was calculated
283 across the fatigue run for each experimental group as the sum of the mean work produced during
284 every second work loop until the muscle was producing less than 50% of the maximal power.
285 Recovery of maximal muscle power output was recorded for 30 minutes, by subjecting the
286 muscle to a set of four sinusoidal length change cycles at 10 minute intervals.

287

288 The experimental protocol was 190 minutes in duration, and control runs were performed
289 regularly to monitor muscle contractile performance over time. After 150 minutes, at the start
290 of the fatigue test, muscle power output had declined by 11% of its maximal value in both
291 soleus and diaphragm. A set of control stimulation and length change parameters were repeated
292 throughout the duration of the experimental procedure to allow all power output values to be
293 corrected to avoid the small decline in muscle quality over time confounding the overall results
294 of the study.

295

296 At the end of these assessments the foil clip, bone and tendons were removed and the remaining
297 muscle blotted on absorbent paper and placed on an electronic balance (Mettler-Toledo B204-
298 S, Greifensee, Switzerland) to determine wet muscle mass to the nearest 0.0001 g. Mean muscle
299 cross-sectional area was calculated from muscle length and mass assuming a density of 1060
300 kg m⁻³ (Mendez and Keys 1960). Maximum isometric muscle stress was calculated as maximal
301 tetanic force divided by mean muscle cross-sectional area (kN m⁻²). Normalised muscle power
302 output was calculated as power output divided by wet muscle mass (W kg⁻¹).

303

304 *Biochemical analysis*

305 We measured activity of lactate dehydrogenase as an indicator of glycolytic capacity, and citrate
306 synthase activity as an indicator of mitochondrial density and oxidative capacity (Larsen et al.,

307 2012). Enzyme activities were determined (in n = 8 animals per treatment) according to
308 published protocols (Seebacher et al., 2003). We determined the activity of sarco-endoplasmic
309 reticulum ATPase (SERCA) as a biochemical indicator of muscle contractile function (in n =
310 8-9 animals per treatment). SERCA re-sequesters Ca²⁺ into the sarcoplasmic reticulum to
311 initiate muscle relaxation so that its activity is related to muscle contractile function (Berchtold
312 et al., 2000). SERCA activity was determined according to published protocols (James et al.,
313 2011).

314

315 Concentrations of myosin heavy chain fast and slow isoforms were determined by capillary
316 electrophoresis in a "Wes" Simple Western system (Protein Simple, Santa Clara, CA, USA)
317 according to the manufacturer's instructions (in n = 5 animals per treatment). We used anti-fast
318 (ab51263) and anti-slow (ab11083) skeletal myosin heavy chain antibodies, and α-tubulin
319 (ab80779) as internal control (Lee et al., 2012) (all from Abcam, Cambridge, MA, USA).

320

321 *Statistical Analysis*

322

323 Mean distance covered during each week of the training protocol was compared between
324 training weeks using a repeated measures ANOVA, with training week as the fixed factor.
325 Pairwise comparisons with Bonferroni correction were used to determine where specific
326 differences occurred. Independent samples t tests were used to examine statistical significance
327 between treatments in whole animal body mass and muscle mass post the treatment
328 intervention. A series of Muscle (2) X Treatment (2) ANOVAs were used to examine the
329 training effect on isometric twitch stress, tetanus stress, maximal work loop power, fatigue,
330 recovery post fatigue, and enzyme activities. Interaction effects were used to determine if the
331 training response was muscle specific. As cumulative work was measured up until the muscle
332 was producing < 50% of its pre fatigue maximal power, the effect of training on this measure
333 was analysed by independent samples t test. For both the trained muscle groups, Pearson's

334 correlation tests were performed to determine the relationship between training volume and
335 muscle contractile performance (i.e tetanus stress, work loop power and time to fatigue).

336

337 We used a three-way ANOVA to test for differences in myosin heavy chain concentrations with
338 Muscle (2) X Treatment (2) X Myosin Isoform (2) as fixed factors. Interaction effects were
339 reported to determine if the training response was muscle specific. All statistical analysis was
340 performed using SPSS (Version 22, SPSS) and significance was determined when P<0.05. Data
341 is represented as mean ± SE.

342

343 The truncated product method (Zaykin et al., 2002) was used to analyse the distribution of *P*-
344 values in this study to provide a *P* value for each group of multiple hypothesis tests to assess
345 the *P*-values were biased via multiple hypothesis testing. The truncated product method *P*-value
346 was 0.0013, for the *Wheel Running, Body Mass & Muscle Mass* group of *P* values, and <0.001,
347 for the *Skeletal Muscle Contractility* group of *P* values, indicating that statistical results were
348 not skewed by multiple hypothesis testing.

349

350

351

352

353

354

355

356

357

358

359

360

361

362 **RESULTS**

363

364 *Wheel Running, Body Mass & Muscle Mass*

365

366 The average weekly distance covered was significantly affected by time (Fig 1. ANOVA p <
367 0.001). Distance covered in week one was significantly lower than in all other weeks (Fig 1.
368 Bonferroni p < 0.02 in all cases). The maximal distance of 5.97 ± 0.29 km was achieved at
369 week two and declined thereafter but was only statistically lower at week 8 (Fig 1; $4.96 \pm$
370 0.31m; Bonferroni p=0.009).

371

372 Post treatment, whole animal body mass of the control group was substantially greater
373 compared to the trained group (52 ± 6 g and 41 ± 1 g for control and trained group respectively; t-
374 test; p=0.028). The body mass of the trained group did not change over the duration of the
375 intervention (T-Test p=0.13).

376

377 Soleus muscle mass was not significantly different between the trained and non-trained group
378 (11 ± 0.08 mg & 11 ± 0.07 mg respectively; T-Test; p = 0.94). As only a section of the diaphragm
379 was taken, which unavoidably differed in size between each extraction, diaphragm mass has
380 not been reported

381

382 *Skeletal Muscle Contractility*

383

384 Following 8 weeks of voluntary wheel running, there was a statistical tendency for maximal
385 isometric twitch stress to be greater in the trained group compared to the control group (Fig 2A.
386 ANOVA p=0.074). Isometric tetanus stress was significantly greater in trained than control
387 mice in both soleus and diaphragm (Fig 2B. ANOVA p<0.001). Time to Half Peak Tetanus
388 (THPT), used as a measure of muscle activation, and Last Stimulus to Half Relaxation (LSHR),
389 used as a measure of relaxation time, were not significantly affected by the training intervention

390 in either soleus or diaphragm (Fig 3A & B. ANOVA $p>0.38$ in both cases). Following the
391 intervention period, soleus and diaphragm work loop power outputs were significantly higher
392 in the trained group compared to controls (Fig 4. ANOVA $p=0.002$) when expressed as power
393 output per muscle mass.

394

395 There was no significant Muscle*Treatment interactions in any of the contractile properties
396 measured (ANOVA $p>0.35$ in all cases).

397

398 *Fatigue*

399

400 Both trained soleus and diaphragm muscles fatigued significantly faster (5.31 ± 0.29 s vs.
401 6.00 ± 0.15 s and 3.56 ± 0.19 s vs. 3.98 ± 0.28 s respectively) than their respective controls (Fig 5 A
402 & B. ANOVA $p=0.034$). There was no significant Muscle*Treatment interaction (Fig 5 A &
403 B. ANOVA $p=0.51$). In comparison to their respective control, the cumulative work over the
404 duration of the fatiguing protocol was significantly greater in trained soleus than control soleus
405 (Fig 5 C. T-Test $p<0.001$). Typical work loop shapes indicate that muscles of the trained group
406 had a greater reduction in net work output (indicated by the area of the work loop) over the
407 duration of the fatigue protocol (Fig 6), when compared with controls. The greater reduction in
408 net work output in the trained group is likely due to a reduction in work done during shortening
409 and greater muscle activity during re-lengthening, possibly due to a slowing of relaxation time,
410 contributing to a greater amount of negative work (net work = positive work during shortening
411 – negative work during lengthening).

412

413 Soleus and diaphragm recovered to 95% of the pre fatigue maximum within 30 minutes of
414 completion of the fatiguing protocol. Recovery was not significantly different between muscles
415 or treatments (ANOVA $p>0.1$ in both cases).

416

417 *Biochemical Analysis*

418

419 No statistically significant Muscle*Treatment interactions were found for LDH, CS, or SERCA
420 activities (Table 2; ANOVA $p>0.5$ in each cases). There was no significant difference between
421 trained and untrained groups for either soleus or diaphragm (Table 2; ANOVA $p>0.2$ in each
422 case).

423

424 There was no statistically significant Muscle*Treatment interaction found in myosin heavy
425 chain isoform concentrations (Table 3; ANOVA $p = 0.34$), and no difference between the
426 trained and untrained groups (Table 3; ANOVA $p = 0.51$). The significant Muscle*Myosin
427 Isoform interaction (Table 3: ANOVA $p=0.04$) shows that diaphragm muscle had greater fast
428 myosin heavy chain concentrations than soleus irrespective of treatment.

429

430

431

432

433

434

435

436

437

438

439

440

441

442

443

444

445

446 **DISCUSSION**

447

448 *Skeletal Muscle Contractility*

449

450 Eight weeks of voluntary wheel running caused a substantial improvement in maximal
451 isometric stress (force normalised to muscle cross-sectional area) and work loop power output
452 (power normalised to muscle mass) of both the soleus and diaphragm muscles in the absence
453 of changes in MHC isoform and metabolic capacity. The present findings are not only the first
454 to demonstrate the value of voluntary wheel running to evoke increased muscle power in
455 isolated muscle, but further indicate the importance of sustained physical activity during early
456 ageing in preventing the age-related increase in body mass and decline in the contractile
457 function of skeletal muscle involved in locomotion or breathing.

458

459 The increase in maximal isometric stress aligns with previous training studies using young
460 healthy rodents (Troup et al., 1986, Carter et al., 1995, Hayes and Williams, 1996). However,
461 unlike the present work using an early ageing model, the changes in contractile performance in
462 young rodents were attributed to altered muscle phenotype and metabolic profile. Although the
463 present findings highlight the value of voluntary wheel running as a method for inducing
464 improvements in contractility in skeletal muscle of mixed fibre type, this may not necessarily
465 apply to muscles composed primarily of fast twitch fibres (Carter et al., 1995, Zhan et al., 1999).

466

467 While the training-induced increase in maximal isometric stress appeared to be greater in the
468 diaphragm compared to soleus (30% and 23% respectively compared to controls), this did not
469 reach statistical significance as there was no Muscle*Treatment interaction for any of the
470 measured contractile variables. There was little difference in the magnitude of the training
471 induced increase in maximal work loop power between the two muscles (26% & 24% for
472 diaphragm and soleus respectively, when compared to controls). Training induced adaptations
473 likely relate to the intensity and duration of muscle recruitment, and as such, the training

474 stimulus could be muscle specific. Given that the response was similar for both muscles, these
475 data indicate that either the training stimulus received was equal, or possibly, that plasticity is
476 greater in one of the examined muscles working at a relatively lower intensity. The latter of
477 would be difficult to assess as traditional methods used to indicate muscle activity during
478 exercise, such as electromyography (EMG), would not be appropriate for the diaphragm.

479

480 *Fatigue Resistance*

481

482 Previous studies evaluating the effect of training on contractility using young healthy rodent
483 models have demonstrated equivocal findings with respect to fatigue resistance (Metzger and
484 Fitts, 1986, Hayes and Williams, 1996, Zhan et al., 1999, Ergen et al., 2005). Such ambiguity
485 can largely be attributed to differences in the experimental procedures, such as training method
486 and duration, muscle tested and contractile parameter measured, making comparison with prior
487 studies difficult. The present study is, however, the first to examine the effect of training on the
488 fatigability of muscle power in an early ageing or ageing model.

489

490 Results of the present work demonstrate that, in comparison to untrained controls, training
491 caused a significant reduction in the ability of both soleus and diaphragm to maintain maximum
492 power output. This may indicate a training induced increase in the force producing capacity of
493 faster fibres within the muscle, and/or a greater disparity between ATP supply and demand
494 given that muscles of the trained group are producing greater force and there are no
495 distinguishable adaptations in regulatory metabolic enzymes. The trained soleus however,
496 produced greater cumulative work over the period of repeated contractions. When considered
497 with respect to *in vivo* function, if both muscles were operating at the same absolute intensity,
498 the trained muscle would have an improved resistance to fatigue by producing the same
499 magnitude of work with a smaller number of recruited fibres, or the same number of fibres
500 working at a relatively lower intensity, due to having an improved maximal power output. With
501 the trained group having a significantly lower body mass compared to controls, the changes in

502 contractility may be more substantial when considered in relation to whole animal locomotor
503 performance. The muscles of the trained group would be working against a reduced whole body
504 inertia, theoretically resulting in a further increased exercise capacity than would be expected
505 by looking at isolated muscle contractility alone.

506

507 The reduction in work done during shortening and increased activation during re-lengthening
508 (as indicated in the typical work loop shapes), over a series of repeated work loop cycles, is
509 indicative of previous studies examining the fatigue response of these muscles using the work
510 loop technique (Tallis et al., 2013, Tallis et al., 2014b). The work loop shapes indicate that these
511 contributors to a reduction in net work, during prolonged cycling of the muscle, were greater
512 in the trained muscles, and thus, may account for the training induced reduction in fatigue
513 resistance.

514

515 *Mechanisms*

516

517 Despite the significant improvement in contractile performance, there were surprisingly no
518 significant training induced changes in LDH, CS or SERCA activities, muscle mass or the
519 concentration of fast and slow MHC isoforms in either soleus or diaphragm muscle. This is
520 particularly interesting given the abundance of literature that demonstrates changes in muscle
521 metabolic profile or a shift in fibre type composition as being the primary cause of skeletal
522 muscle adaptations to training (Sullivan et al., 1995, Allen et al., 2001, Sugiura et al., 1992).
523 The prevalence and magnitude of such mechanistic changes are likely to be specific to the
524 muscle studied and the intensity and duration of the training intervention.

525

526 In line with the present results, a small number of studies have demonstrated training induced
527 improvements in skeletal muscle contractility in young animal models that have not always
528 been associated with changes in phenotype expression (Taylor et al., 1976, Carter et al., 1995,
529 Zhan et al., 1999). In agreement with the present study, Sullivan et al. (1995) reported that,

530 training failed to elicit any change in the MHC profile of soleus muscle in young and old rats,
531 and further indicated a muscle and age specific continuum of adaptations relating to exercise
532 intensity.

533

534 Although some studies indicate that training induced changes in skeletal muscle metabolic
535 capacity appear to occur much more readily (Allen et al., 2001, Zhan et al., 1999, Ergen et al.,
536 2005), other evidence denotes that this may not always be the case. Allen et al. (2001) reported
537 that 4 weeks voluntary wheel running caused a significant increase in the oxidative capacity of
538 mouse tibialis anterior and a greater expression of type IIa and IId/x fibres. Interestingly the
539 metabolic capacity of gastrocnemius was unchanged and although greater expression of type
540 IIa and IId/x fibres was demonstrated after 2 weeks, this was not maintained after 4 weeks of
541 training.

542

543 Much of the evidence outlining training-induced adaptations in fibre type and metabolic
544 capacity comes from studies using healthy young muscle (Allen et al., 2001, Zhan et al., 1999,
545 Ergen et al., 2005) and although there is evidence of a similar method of adaptation in older
546 adults (Menshikova et al., 2006, Flack et al., 2016) this has been explored in less detail.
547 Irrespective of the previous literature, the present data infer that these mechanisms are not the
548 primary cause of training induced adaptations in skeletal muscle contractility that arise
549 following prolonged low intensity exercise in mixed fibre type skeletal muscle undergoing the
550 early stages of age related degeneration. Although the present study demonstrates a substantial
551 increase in muscle contractility, these findings may suggest an age-related reduction in skeletal
552 muscle plasticity which may limit the rate and magnitude of adaptations that can occur during
553 training.

554

555 Animals in the training group had a significantly lower body mass than the control group and
556 it may be that a subsequent infiltration of lipid into the muscle of control animals, may
557 contribute to the difference in contractile performance between the control and trained group.

558 Recent work has demonstrated a link between muscular lipid accumulation and a reduction in
559 the isometric stress and normalised work loop power of isolated skeletal muscle (Ciapaite et
560 al., 2015, Tallis et al., 2017). Akhmedov and Berdeaux (2013) concluded that excessive
561 accumulation of skeletal muscle lipids affects the ability of muscle to maintain and regenerate
562 contractile proteins. The improvement in the contractile performance of the muscles of the
563 trained group may in part be attributed to the effectiveness of exercise in weight management.

564

565 The age related reduction in contractile performance has, in part, previously been attributed to
566 a reduction in the effectiveness of the Ca^{2+} handling process (Larsson and Salviati, 1989). Given
567 that no difference was apparent in the isometric activation and relaxation times or SERCA
568 between the trained and the untrained group, it is unlikely that training was unable to
569 substantially reverse these effects. However, an improvement in the efficiency of cross bridge
570 kinetics may occur independently of changes in Ca^{2+} handling, and this may account for the
571 training induced increase in force and power demonstrated in this study. Future work should
572 look to establish the effects of training on rate limiting enzymes and structural proteins such as
573 myosin light chain, myosin ATPase and troponin isoforms that could influence the ability of
574 muscle to produce force.

575

576 *Voluntary Wheel Running*

577

578 Mice in the current study ran a daily average of $5.97 \pm 0.29\text{km}$, which is slightly lower than the
579 6.8 km reported by Allen et al. (2001) in 10 week old mice. Despite the significant improvement
580 in skeletal muscle contractility in the present study, the distance covered by wheel running mice
581 had significantly decreased during the latter stages of the wheel running intervention. This is
582 particularly interesting given that a positive training response should theoretically promote
583 further running distances. The animals, therefore, may not be at the peak of their ‘trained’ state
584 after the 8 week intervention. This may arise from a problem with an inability to self-regulate
585 a progressive training program, or more likely the effects of increasing age. These findings

586 indicate that a training-induced increase in the contractile performance of skeletal muscle
587 cannot fully offset the deterioration in muscle contractility that occurs during the early onset of
588 the ageing process. It would be of interest to compare the current results with those obtained
589 using a protocol of treadmill running, where exercise volume and intensity can be more
590 precisely regulated and could be gradually altered over time.

591

592 However, it is interesting to note that there was no relationship between training volume and
593 muscle function in either the soleus or diaphragm muscles. However, it is acknowledged that,
594 in future work, individual responses need to be analysed using a larger sample size.

595

596 *Limitations*

597

598 Although the work loop technique provides a better approximation of real world muscle
599 function, the length change waveforms used *in vivo* are likely to be more complex than the
600 sinusoidal pattern used in the present study (James et al 1995; Dickinson et al., 2000).
601 Furthermore, the pattern of fibre stimulation and length change waveforms are likely to be
602 manipulated throughout movement (Wakeling and Rozitis, 2005), particularly during repeated
603 contractions in order to minimise the build-up in work done on the muscle during muscle
604 lengthening (Tallis et al., 2013).

605

606 The results of the present study offer an important insight into the effects of voluntary wheel
607 running on both the soleus and diaphragm, however these results may not be generalizable to
608 other locomotory muscles. Future work should also consider the effect of voluntary wheel
609 running on hip and knee extensor muscles given the substantial role of such muscle groups in
610 walking and running.

611

612 *Practical Implications*

613

614 The present findings show the value of low intensity, high frequency activity on skeletal muscle
615 contractile performance and indicate that such exercise modalities would be beneficial for
616 slowing the loss in skeletal muscle contractility that occurs during early ageing. Importantly,
617 maintaining a greater muscle function during this time may be significant for offsetting the
618 more substantial decline in skeletal muscle contractile performance that occurs during older
619 ageing. The extensive improvement in the contractile performance of the diaphragm is likely
620 to play an important role in the training induced improvement in pulmonary function. Improved
621 pulmonary function could be important for mediating further exercise induced enhancements
622 in muscle contractility by satisfying the increased skeletal muscle oxygen demand,
623 consequently promoting a greater exercise capacity.

624

625 *Conclusion*

626

627 The present study demonstrates that eight weeks of voluntary wheel running caused significant
628 improvements in isolated skeletal muscle contractility in mice undergoing early ageing. The
629 results indicate that the increase in muscle contractile performance occurs without significant
630 changes in muscle mass, fibre type or metabolic capacity, in contrast to the findings
631 demonstrated in younger trained muscle. Such findings support the value of physical activity
632 in slowing the early age related decline in muscle contractile performance. Despite the given
633 increase in contractility, the present work infers that voluntary wheel running is not sufficient
634 in fully offsetting the degeneration of muscle contractile performance that occurs during early
635 ageing. Future work focusing on changes in the effectiveness of cross bridge formation and
636 mechanisms related to the obesity associated reduction in muscle contractility may be important
637 in identifying the primary mechanisms causing an improved contractile performance following
638 training during the onset of the skeletal muscle ageing response.

639

640

641

642 **ACKNOWLEDGEMENTS**

643 Thank you to Roy Petticrew, Mark Bodycote & Bethan Grist for technical assistance.

644

645

646

647

648

649

650

651

652

653

654

655

656

657

658

659

660

661

662

663

664

665

666

667

668

669

670 **TABLES****Table 1. Relationship between total wheel running distance and muscle contractile performance**

		Maximal Tetanus Stress (kN ⁻²)	Work Loop Power (W/kg)	Time to Fatigue (s)
Trained DIA	<i>R</i>	0.102	0.102	-0.348
	<i>P</i>	0.827	0.828	0.444
Trained SOL	<i>R</i>	0.069	-0.438	-0.379
	<i>P</i>	0.883	0.325	0.401

[*N=7 in each case*]

671

672

673

674

675

676

677

678

679

680

681

682

683

684

685

686

687

688

689

Table 2. The effect of 8 weeks of voluntary wheel running on soleus and diaphragm muscle LDH, CS & SERCA activities

	Soleus		Diaphragm	
	<i>Control</i>	<i>Trained</i>	<i>Control</i>	<i>Trained</i>
LDH ($\mu\text{mol mg}^{-1}$ tissue min^{-1})	90.4 \pm 10.4	82.4 \pm 12.6	149.9 \pm 20.5	135.2 \pm 15
CS ($\mu\text{mol g}^{-1}$ tissue min^{-1})	23 \pm 7	16.8 \pm 1.8	87.2 \pm 7.4	71.8 \pm 12
SERCA ($\mu\text{mol mg}^{-1}$ tissue h^{-1})	1.7 \pm .6	2.87 \pm 0.9	6.3 \pm 2.5	2.6 \pm 0.41

690 [Data represented as mean \pm s.e.; N=7 in each case]

691

692

693

694

695

696

697

698

699

700

701

702

703

704

705

706

Table 3. The effect of 8 weeks of voluntary wheel running on soleus and diaphragm fast and slow myosin heavy chain concentration (normalized to alpha tubulin)

	Soleus		Diaphragm	
	<i>Control</i>	<i>Trained</i>	<i>Control</i>	<i>Trained</i>
Slow Myosin	0.108±0.026	0.16±0.037	0.1±0.026	0.132±0.032
Fast Myosin	0.063±0.02	0.094±0.052	0.195±0.057	0.148±0.045

707 [Data represented as mean ± s.e.; N=5 in each case]

708

709

710

711

712

713

714

715

716

717

718

719

720

721

722

723

724

725

726

727

728 **FIGURES**

729 Figure 1 – Average daily (white squares) and weekly (black circles and line) mean distance
730 covered during 8 weeks voluntary wheel running in 38 week old CD1 female mice [Data
731 represented as mean \pm s.e.; N=14]

732

733 Figure 2 – The effects of 8 weeks voluntary wheel running on the maximal isometric twitch (A)
734 and tetanus stress (force normalised to muscle cross-sectional area) (B) of mouse soleus and
735 diaphragm muscle [Data represented as mean \pm s.e.; N=7 in each case; * indicate statistical
736 differences between trained and control groups]

737

738 Figure 3 – The effects of 8 weeks voluntary wheel running on Time to Half Peak Tetanus
739 (THPT; A) and Last Stimulus to Half Relaxation (LSHR; B) in mouse soleus and diaphragm
740 muscle [Data represented as mean \pm s.e.; N=7 in each case]

741

742 Figure 4 – The effects of 8 weeks voluntary wheel running on the maximal work loop power
743 output (normalised to muscle mass) of mouse soleus and diaphragm muscle [Data represented
744 as Mean \pm s.e.; N=7 in each case; * indicate statistical differences between trained and control
745 groups]

746

747 Figure 5 – The effects of 8 weeks voluntary wheel running on the fatigue of muscle power
748 output (A & B) and the cumulative net work during the fatigue protocol (C) in mouse soleus
749 muscle respectively [CS = Control Soleus; TS = Trained Soleus; CD = Control Diaphragm; TD
750 = Trained Diaphragm; Data represented as Mean \pm s.e.; N=7 in each case]

751

752 Figure 6. Typical work loop shapes for control and trained soleus (A & B) and diaphragm (C
753 & D) [Start of arrow indicates L_0 and direction of lengthening; 0.4s, 2.48, and 5.2s represent
754 time since the start of the fatigue protocol for the soleus; 0.3s, 2.0, and 3.7s represent time
755 since the start of the fatigue protocol for the diaphragm]

756 **REFERENCES**

- 757 AKHMEDOV, D. & BERDEAUX, R. 2013. The effects of obesity on skeletal muscle regeneration.
758 *Front Physiol*, 4, 371.
- 759 ALLEN, D. L., HARRISON, B. C., MAASS, A., BELL, M. L., BYRNES, W. C. & LEINWAND, L.
760 A. 2001. Cardiac and skeletal muscle adaptations to voluntary wheel running in the mouse. *J
761 Appl Physiol (1985)*, 90, 1900-8.
- 762 ALTRINGHAM, J. D. & YOUNG, I. S. 1991. Power output and the frequency of oscillatory work in
763 mammalian diaphragm muscle: the effects of animal size. *J Exp Biol*, 157, 381-9.
- 764 ASKEW, G. N. & MARSH, R. L. 1997. The effects of length trajectory on the mechanical power
765 output of mouse skeletal muscles. *J Exp Biol*, 200, 3119-31.
- 766 BEHNKE, B. J., RAMSEY, M. W., STABLEY, J. N., DOMINGUEZ, J. M., 2ND, DAVIS, R. T.,
767 3RD, MCCULLOUGH, D. J., MULLER-DELP, J. M. & DELP, M. D. 2012. Effects of aging
768 and exercise training on skeletal muscle blood flow and resistance artery morphology. *J Appl
769 Physiol (1985)*, 113, 1699-708.
- 770 BERCHTOLD, M. W., BRINKMEIER, H. & MUNTENER, M. 2000. Calcium ion in skeletal muscle:
771 its crucial role for muscle function, plasticity, and disease. *Physiol Rev*, 80, 1215-65.
- 772 BROOKS, S. V. & FAULKNER, J. A. 1988. Contractile properties of skeletal muscles from young,
773 adult and aged mice. *J Physiol*, 404, 71-82.
- 774 BROWN, M., ROSS, T. P. & HOLLOSZY, J. O. 1992. Effects of ageing and exercise on soleus and
775 extensor digitorum longus muscles of female rats. *Mech Ageing Dev*, 63, 69-77.
- 776 CARTER, G. T., WINEINGER, M. A., WALSH, S. A., HORASEK, S. J., ABRESCH, R. T. &
777 FOWLER, W. M., JR. 1995. Effect of voluntary wheel-running exercise on muscles of the
778 mdx mouse. *Neuromuscul Disord*, 5, 323-32.
- 779 CIAPAITE, J., VAN DEN BERG, S. A., HOUTEN, S. M., NICOLAY, K., VAN DIJK, K. W. &
780 JENESON, J. A. 2015. Fiber-type-specific sensitivities and phenotypic adaptations to dietary
781 fat overload differentially impact fast- versus slow-twitch muscle contractile function in
782 C57BL/6J mice. *J Nutr Biochem*, 26, 155-64.
- 783 DICKINSON, M. H., FARLEY, C. T., FULL, R. J., KOEHL, M. A., KRAM, R. & LEHMAN, S.
784 2000. How animals move: an integrative view. *Science*, 288, 100-6.
- 785 DOHERTY, T. J. 2003. Invited review: Aging and sarcopenia. *J Appl Physiol (1985)*, 95, 1717-27.
- 786 ERGEN, N., KURDAK, H., ERDOGAN, S., METE, U. O., KAYA, M., DIKMEN, N., DOGAN, A. &
787 KURDAK, S. S. 2005. The effects of aerobic exercise on skeletal muscle metabolism,
788 morphology and in situ endurance in diabetic rats. *J Sports Sci Med*, 4, 472-81.
- 789 FLACK, K. D., DAVY, B. M., DEBERARDINIS, M., BOUTAGY, N. E., MCMILLAN, R. P.,
790 HULVER, M. W., FRISARD, M. I., ANDERSON, A. S., SAVLA, J. & DAVY, K. P. 2016.
791 Resistance exercise training and in vitro skeletal muscle oxidative capacity in older adults.
792 *Physiol Rep*, 4.
- 793 GONZALEZ, E., MESSI, M. L. & DELBONO, O. 2000. The specific force of single intact extensor
794 digitorum longus and soleus mouse muscle fibers declines with aging. *J Membr Biol*, 178,
795 175-83.
- 796 HAYES, A. & WILLIAMS, D. A. 1996. Beneficial effects of voluntary wheel running on the
797 properties of dystrophic mouse muscle. *J Appl Physiol (1985)*, 80, 670-9.
- 798 HIGGINS, M. F., JAMES, R. S. & PRICE, M. J. 2013. The effects of sodium bicarbonate (NaHCO₃)
799 ingestion on high intensity cycling capacity. *J Sports Sci*, 31, 972-81.
- 800 HOULE-LEROY, P., GARLAND, T., JR., SWALLOW, J. G. & GUDERLEY, H. 2000. Effects of
801 voluntary activity and genetic selection on muscle metabolic capacities in house mice *Mus
802 domesticus*. *J Appl Physiol (1985)*, 89, 1608-16.
- 803 IOLASCON, G., DI PIETRO, G., GIMIGLIANO, F., MAURO, G. L., MORETTI, A., GIAMATTEI,
804 M. T., ORTOLANI, S., TARANTINO, U. & BRANDI, M. L. 2014. Physical exercise and
805 sarcopenia in older people: position paper of the Italian Society of Orthopaedics and Medicine
806 (OrtoMed). *Clin Cases Miner Bone Metab*, 11, 215-21.
- 807 JAMES, R. S., ALTRINGHAM, J. D. & GOLDSPINK, D. F. 1995. The mechanical properties of fast
808 and slow skeletal muscles of the mouse in relation to their locomotory function. *J Exp Biol*,
809 198, 491-502.
- 810 JAMES, R. S., KOHLSDORF, T., COX, V. M. & NAVAS, C. A. 2005. 70 microM caffeine treatment
811 enhances in vitro force and power output during cyclic activities in mouse extensor digitorum
812 longus muscle. *Eur J Appl Physiol*, 95, 74-82.

- 813 JAMES, R. S., WALTER, I. & SEEBACKER, F. 2011. Variation in expression of calcium-handling
814 proteins is associated with inter-individual differences in mechanical performance of rat
815 (Rattus norvegicus) skeletal muscle. *J Exp Biol*, 214, 3542-8.
- 816 JAMES, R. S., YOUNG, I. S., COX, V. M., GOLDSPINK, D. F. & ALTRINGHAM, J. D. 1996.
817 Isometric and isotonic muscle properties as determinants of work loop power output. *Pflugers
818 Arch*, 432, 767-74.
- 819 JOSEPHSON, R. K. 1985. Mechanical power output from striated muscle during cyclical contraction.
820 *Journal of Experimental Biology*, 114, 493-512.
- 821 LANDI, F., LIPEROTI, R., RUSSO, A., GIOVANNINI, S., TOSATO, M., CAPOLUONGO, E.,
822 BERNABEI, R. & ONDER, G. 2012. Sarcopenia as a risk factor for falls in elderly
823 individuals: results from the iSIRENTE study. *Clin Nutr*, 31, 652-8.
- 824 LARSEN, S., NIELSEN, J., HANSEN, C. N., NIELSEN, L. B., WIBRAND, F., STRIDE, N.,
825 SCHRODER, H. D., BOUSHEL, R., HELGE, J. W., DELA, F. & HEY-MOGENSEN, M.
826 2012. Biomarkers of mitochondrial content in skeletal muscle of healthy young human
827 subjects. *J Physiol*, 590, 3349-60.
- 828 LARSSON, L. & SALVIATI, G. 1989. Effects of age on calcium transport activity of sarcoplasmic
829 reticulum in fast- and slow-twitch rat muscle fibres. *J Physiol*, 419, 253-64.
- 830 LEE, I., HUTTEMANN, M., LIU, J., GROSSMAN, L. I. & MALEK, M. H. 2012. Deletion of heart-
831 type cytochrome c oxidase subunit 7a1 impairs skeletal muscle angiogenesis and oxidative
832 phosphorylation. *J Physiol*, 590, 5231-43.
- 833 LEXELL, J. 1995. Human aging, muscle mass, and fiber type composition. *J Gerontol A Biol Sci Med
834 Sci*, 50 Spec No, 11-6.
- 835 MARCELL, T. J. 2003. Sarcopenia: causes, consequences, and preventions. *J Gerontol A Biol Sci Med
836 Sci*, 58, M911-6.
- 837 MAYER, F., SCHARHAG-ROSENBERGER, F., CARLOSOHN, A., CASSEL, M., MÜLLER, S. &
838 SCHARHAG, J. 2011. The intensity and effects of strength training in the elderly. *Dtsch
839 Arztebl Int*, 108, 359-64.
- 840 MCCARTNEY, N., HICKS, A. L., MARTIN, J. & WEBBER, C. E. 1995. Long-term resistance
841 training in the elderly: effects on dynamic strength, exercise capacity, muscle, and bone. *J
842 Gerontol A Biol Sci Med Sci*, 50, B97-104.
- 843 MELOV, S., TARNOPOLSKY, M. A., BECKMAN, K., FELKEY, K. & HUBBARD, A. 2007.
844 Resistance exercise reverses aging in human skeletal muscle. *PLoS One*, 2, e465.
- 845 MENSHIKOVA, E. V., RITOV, V. B., FAIRFULL, L., FERRELL, R. E., KELLEY, D. E. &
846 GOODPASTER, B. H. 2006. Effects of exercise on mitochondrial content and function in
847 aging human skeletal muscle. *J Gerontol A Biol Sci Med Sci*, 61, 534-40.
- 848 METZGER, J. M. & FITTS, R. H. 1986. Contractile and biochemical properties of diaphragm: effects
849 of exercise training and fatigue. *J Appl Physiol* (1985), 60, 1752-8.
- 850 NICOLOPOULOS-STOURNARAS, S. & ILES, J. F. 1984. Hind limb muscle activity during
851 locomotion in the rat. *Journal of Zoology*, 203, 427-440.
- 852 PYKA, G., LINDENBERGER, E., CHARETTE, S. & MARCUS, R. 1994. Muscle strength and fiber
853 adaptations to a year-long resistance training program in elderly men and women. *J Gerontol,
854 49*, M22-7.
- 855 REID, K. F., CALLAHAN, D. M., CARABELLO, R. J., PHILLIPS, E. M., FRONTERA, W. R. &
856 FIELDING, R. A. 2008. Lower extremity power training in elderly subjects with mobility
857 limitations: a randomized controlled trial. *Aging Clin Exp Res*, 20, 337-43.
- 858 REID, K. F., MARTIN, K. I., DOROS, G., CLARK, D. J., HAU, C., PATTEN, C., PHILLIPS, E. M.,
859 FRONTERA, W. R. & FIELDING, R. A. 2015. Comparative effects of light or heavy
860 resistance power training for improving lower extremity power and physical performance in
861 mobility-limited older adults. *J Gerontol A Biol Sci Med Sci*, 70, 374-80.
- 862 SEEBACKER, F., GUDERLEY, H., ELSEY, R. M. & TROSCLAIR, P. L., 3RD 2003. Seasonal
863 acclimatisation of muscle metabolic enzymes in a reptile (*Alligator mississippiensis*). *J Exp
864 Biol*, 206, 1193-200.
- 865 SEGUIN, R. & NELSON, M. E. 2003. The benefits of strength training for older adults. *Am J Prev
866 Med*, 25, 141-9.
- 867 SHEEL, A. W. 2002. Respiratory muscle training in healthy individuals: physiological rationale and
868 implications for exercise performance. *Sports Med*, 32, 567-81.
- 869 SUGIURA, T., MORIMOTO, A. & MURAKAMI, N. 1992. Effects of endurance training on myosin
870 heavy-chain isoforms and enzyme activity in the rat diaphragm. *Pflugers Arch*, 421, 77-81.

- 871 SULLIVAN, V. K., POWERS, S. K., CRISWELL, D. S., TUMER, N., LAROCHELLE, J. S. &
872 LOWENTHAL, D. 1995. Myosin heavy chain composition in young and old rat skeletal
873 muscle: effects of endurance exercise. *J Appl Physiol* (1985), 78, 2115-20.
- 874 TALLIS, J., HIGGINS, M. F., COX, V. M., DUNCAN, M. J. & JAMES, R. S. 2014a. Does a
875 physiological concentration of taurine increase acute muscle power output, time to fatigue,
876 and recovery in isolated mouse soleus (slow) muscle with or without the presence of caffeine?
877 *Can J Physiol Pharmacol*, 92, 42-9.
- 878 TALLIS, J., HILL, C., JAMES, R. S., COX, V. M. & SEEBACHER, F. 2017. The effect of obesity on
879 the contractile performance of isolated mouse soleus, EDL, and diaphragm muscles. *J Appl*
880 *Physiol* (1985), 122, 170-181.
- 881 TALLIS, J., JAMES, R. S., COX, V. M. & DUNCAN, M. J. 2012. The effect of physiological
882 concentrations of caffeine on the power output of maximally and submaximally stimulated
883 mouse EDL (fast) and soleus (slow) muscle. *J Appl Physiol* (1985), 112, 64-71.
- 884 TALLIS, J., JAMES, R. S., COX, V. M. & DUNCAN, M. J. 2013. The effect of a physiological
885 concentration of caffeine on the endurance of maximally and submaximally stimulated mouse
886 soleus muscle. *J Physiol Sci*, 63, 125-32.
- 887 TALLIS, J., JAMES, R. S., LITTLE, A. G., COX, V. M., DUNCAN, M. J. & SEEBACHER, F. 2014b.
888 Early effects of ageing on the mechanical performance of isolated locomotory (EDL) and
889 respiratory (diaphragm) skeletal muscle using the work-loop technique. *Am J Physiol Regul*
890 *Integr Comp Physiol*, 307, R670-84.
- 891 TAYLOR, R. G., FOWLER, W. M., JR. & DOERR, L. 1976. Exercise effect on contractile properties
892 of skeletal muscle in mouse muscular dystrophy. *Arch Phys Med Rehabil*, 57, 174-80.
- 893 TROUP, J. P., METZGER, J. M. & FITTS, R. H. 1986. Effect of high-intensity exercise training on
894 functional capacity of limb skeletal muscle. *J Appl Physiol* (1985), 60, 1743-51.
- 895 WAKELING, J. M. & ROZITIS, A. I. 2005. Motor unit recruitment during vertebrate locomotion.
896 *Journal of Animal Biology*, 55, 41-58.
- 897 WHO 2017. Physical Activity and Older Adults.
- 898 WILLEMS, M. E. & STAUBER, W. T. 2000. Effect of resistance training on muscle fatigue and
899 recovery in intact rats. *Med Sci Sports Exerc*, 32, 1887-93.
- 900 WILLIAMS, G. N., HIGGINS, M. J. & LEWEK, M. D. 2002. Aging skeletal muscle: physiologic
901 changes and the effects of training. *Phys Ther*, 82, 62-8.
- 902 WOO, T., YU, S. & VISVANATHAN, R. 2016. Systematic Literature Review on the Relationship
903 Between Biomarkers of Sarcopenia and Quality of Life in Older People. *J Frailty Aging*, 5,
904 88-99.
- 905 ZHAN, W. Z., SWALLOW, J. G., GARLAND, T., JR., PROCTOR, D. N., CARTER, P. A. & SIECK,
906 G. C. 1999. Effects of genetic selection and voluntary activity on the medial gastrocnemius
907 muscle in house mice. *J Appl Physiol* (1985), 87, 2326-33.
- 908 ZHANG, Y. L. & KELSEN, S. G. 1990. Effects of aging on diaphragm contractile function in golden
909 hamsters. *Am Rev Respir Dis*, 142, 1396-401.
- 910

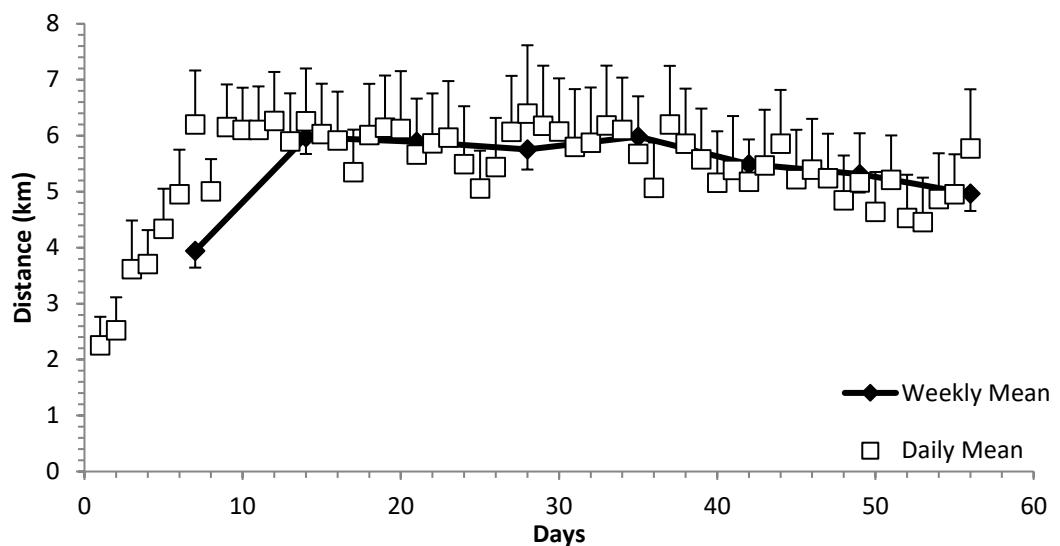


Figure 1

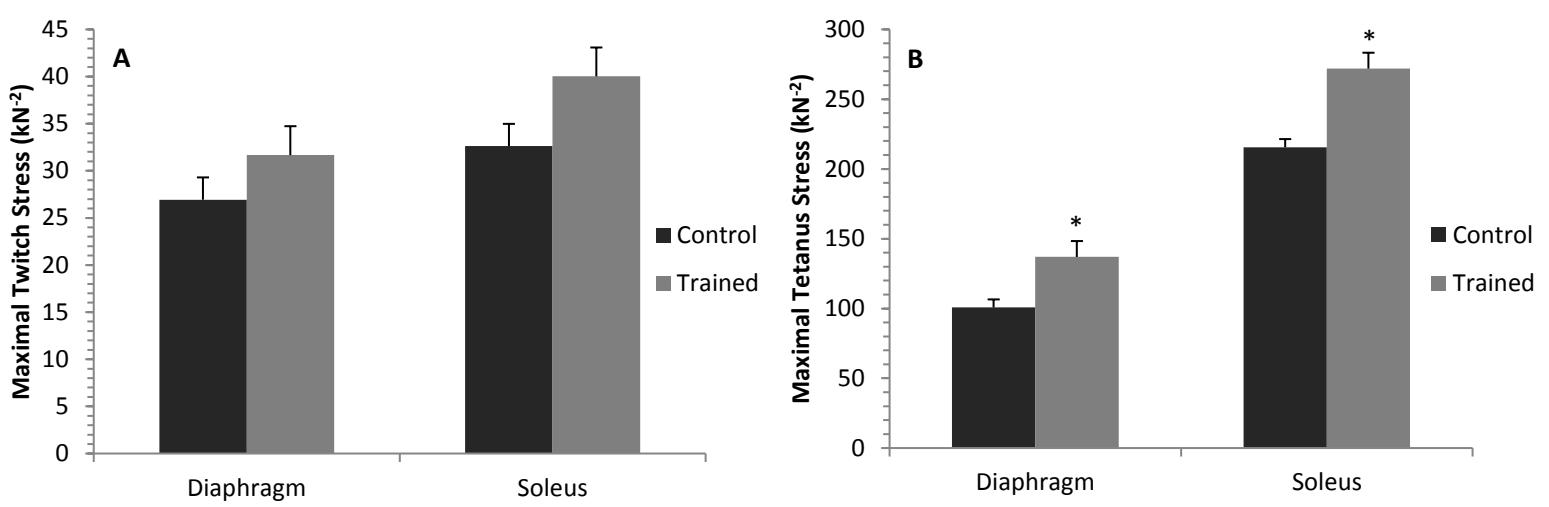


Figure 2

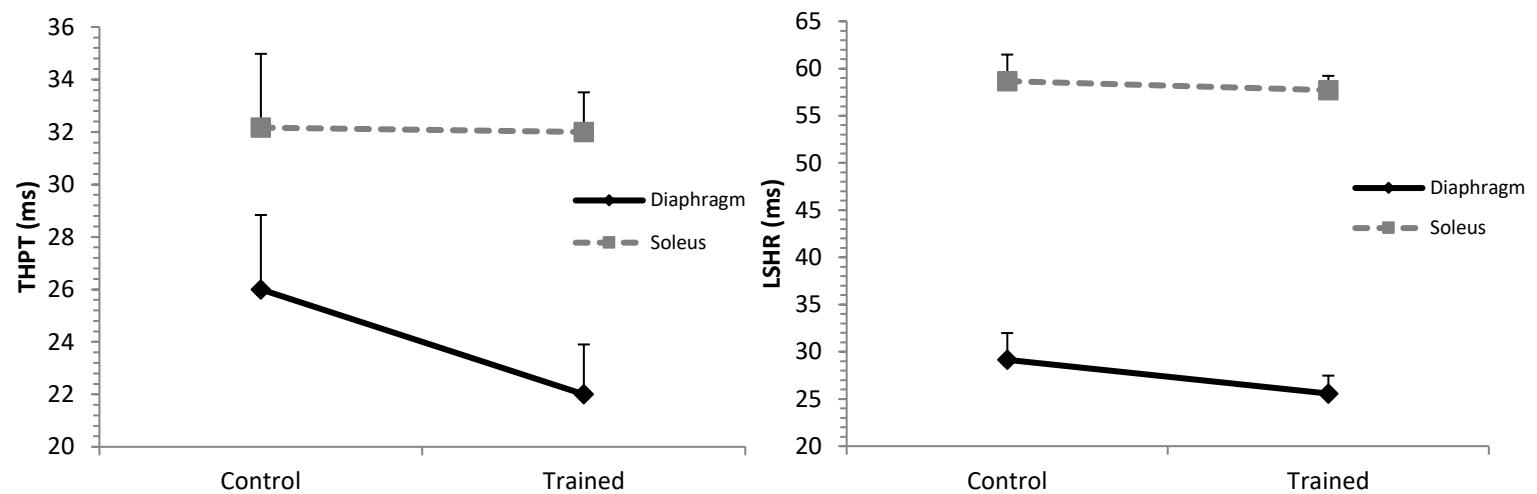


Figure 3

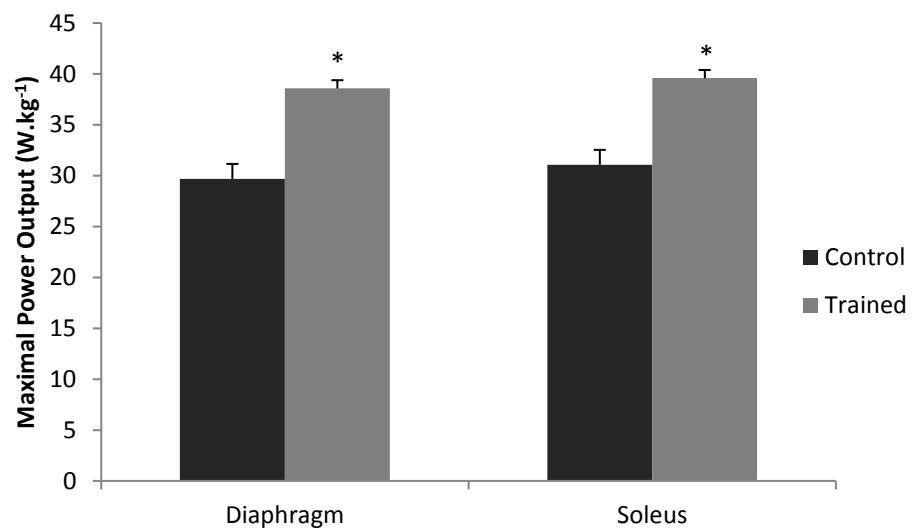


Figure 4

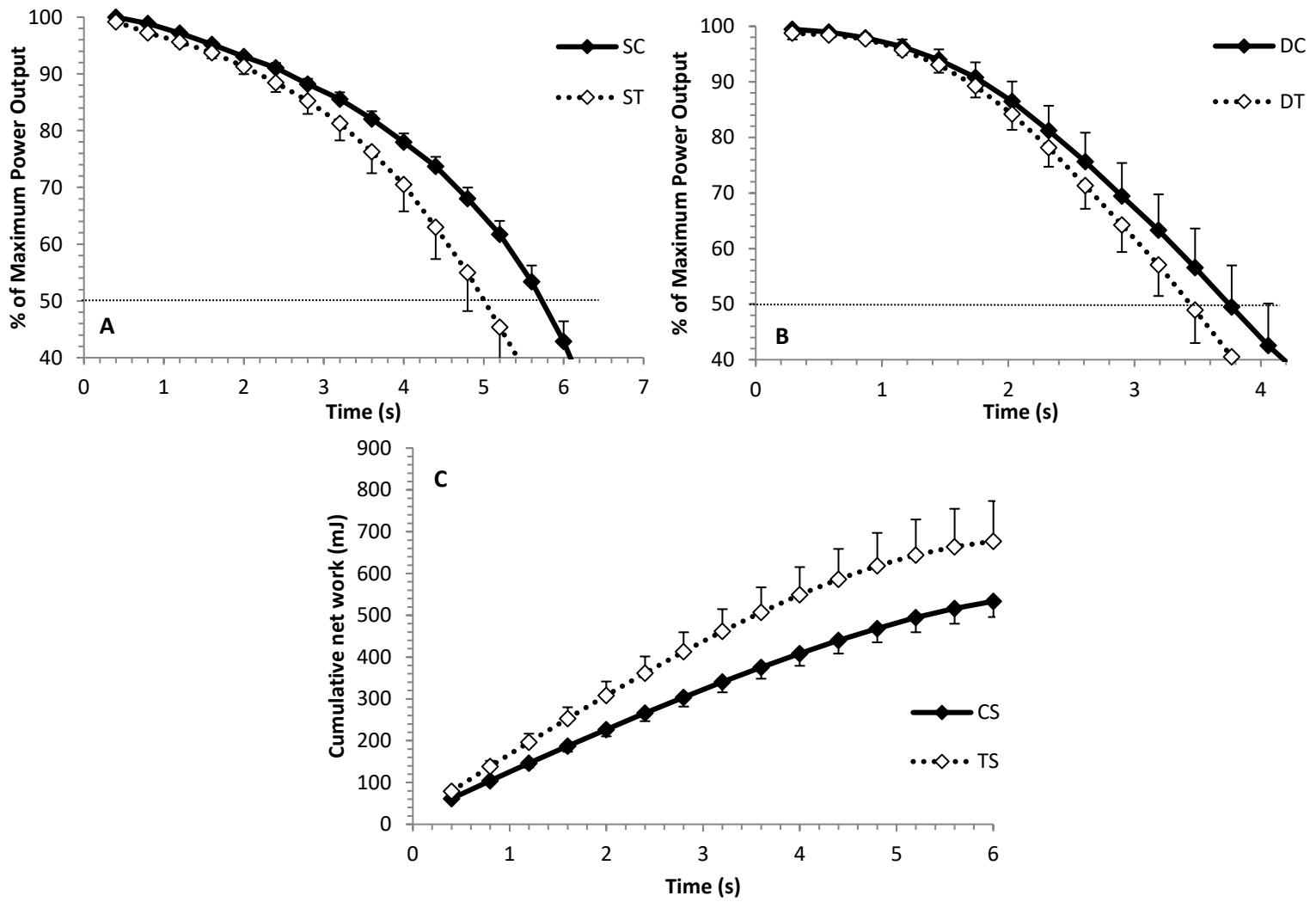


Figure 5

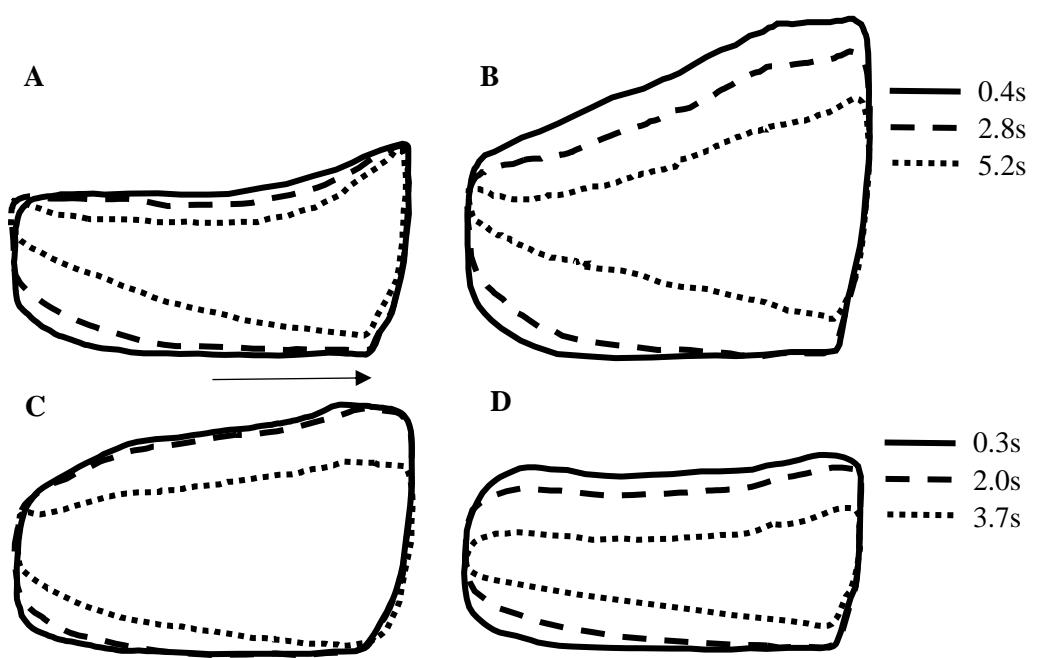


Figure 6.